

PATENT COOPERATION TREATY

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INTERNATIONAL SEARCH REPORT

(PCT Article 18 and Rules 43 and 44)

Applicant's or agent's file reference P-1999-014-2	<div style="display: flex; justify-content: space-between;"> <div style="text-align: center;">FOR FURTHER ACTION</div> <div style="font-size: small;">see Notification of Transmittal of International Search Report (Form PCT/ISA/220) as well as, where applicable, item 5 below.</div> </div>	
International application No. PCT/DK 00/00380	International filing date (<i>day/month/year</i>) 7 July 2000	(Earliest) Priority Date (<i>day/month/year</i>) 6 May 1999
Applicant Oticon A/S et al.		

This international search report has been prepared by this International Searching Authority and is transmitted to the applicant according to Article 18. A copy is being transmitted to the International Bureau.

This international search report consists of a total of 3 sheets.

☒ It is also accompanied by a copy of each prior art document cited in this report.

1. ☐ Certain claims were found unsearchable (See Box I).

2. ☐ Unity of invention is lacking (See Box II).

3. ☐ The international application contains disclosure of a nucleotide and/or amino acid sequence listing and the international search was carried out on the basis of the sequence listing

☐ filed with the international application.
☐ furnished by the applicant separately from the international application,

☐ but not accompanied by a statement to the effect that it did not include matter going beyond the disclosure in the international application as filed.

☐ transcribed by this Authority.

4. With regard to the title, ☒ the text is approved as submitted by the applicant.
☐ the text has been established by this Authority to read as follows:

5. With regard to the abstract,

☒ the text is approved as submitted by the applicant.
☐ the text has been established, according to Rule 38.2(b), by this Authority as it appears in Box III. The applicant may, within one month from the date of mailing of this international search report, submit comments to this Authority.

6. The figure of the drawings to be published with the abstract is:

Figure No. 1

☒ as suggested by the applicant.
☐ because the applicant failed to suggest a figure.
☐ because this figure better characterizes the invention.

☐ None of the figures.

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INTERNATIONAL SEARCH REPORT

International application No.

PCT/DK 00/00380

A. CLASSIFICATION OF SUBJECT MATTER

IPC7: H04R 25/00, G10L 21/02

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC7: G10L, H04R

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 5661814 A (A.N KÄLIN ET AL.), 26 August 1997 (26.08.97), column 1, line 50 - line 67; column 13, line 19 - line 61, claim 31 --	1-13
X	EP 0579152 A1 (MINNESOTA MINING AND MANUFACTURING COMPANY), 19 January 1994 (19.01.94), column 2, line 8 - line 26; column 11, line 10 - column 12, line 41; column 12, line 50 - column 13, line 19 --	1-13
A	US 5259033 A (R.L.A. GOODINGS ET AL.), 2 November 1993 (02.11.93), column 3, line 14 - line 25, abstract --	1-13

☒ Further documents are listed in the continuation of Box C.☒ See patent family annex.

* Special categories of cited documents:

- "A" document defining the general state of the art which is not considered to be of particular relevance
- "E" earlier document but published on or after the international filing date
- "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
- "O" document referring to an oral disclosure, use, exhibition or other means
- "P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance: the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"Y" document of particular relevance: the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art

"&" document member of the same patent family

Date of the actual completion of the international search

16 October 2000

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C (Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US 5016280 A (A.M. ENGBRETSON ET AL.), 14 May 1991 (14.05.91), column 8, line 50 - column 9, line 25; column 12, line 67 - column 13, line 17 --	1-13
A	US 5835607 A (R. MARTIN ET AL.), 10 November 1998 (10.11.98), column 4, line 29 - column 5, line 60 -- -----	1-13

INTERNATIONAL SEARCH REPORT
Information on patent family members

A 291626

03/10/00

International application No.

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Patent document cited in search report			Publication date	Patent family member(s)		Publication date
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				WO	9507597 A	16/03/95

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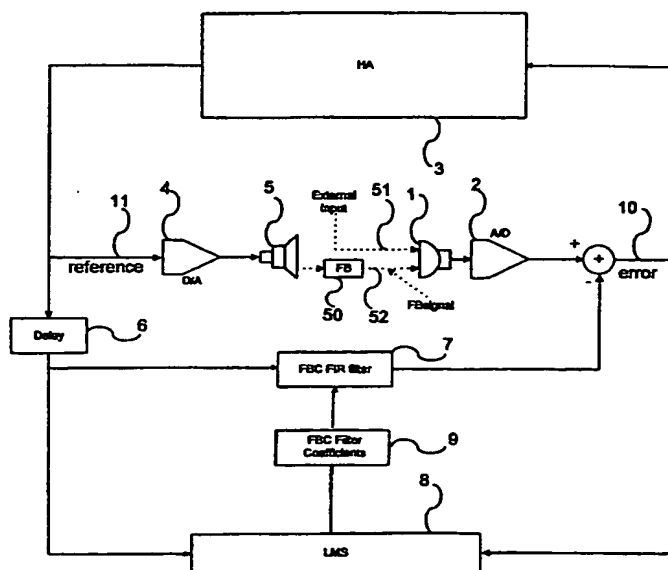
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A/S [DK/DK]; Strandvejen 58, DK-2900 Hellerup (DK).</p> <p>(72) Inventors; and</p> <p>(75) Inventors/Applicants (<i>for US only</i>): NIELSEN, Jakob
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[Continued on next page]

- (54) Title: FEEDBACK CANCELLATION WITH LOW FREQUENCY INPUT**



(57) Abstract: The invention relates to a method for canceling feedback in an acoustic system comprising a microphone, a signal path, a speaker and means for detecting presence of feedback between the speaker and the microphone, the method comprising using a LMS algorithm for generating filter coefficients and using a highpass filter to prevent low-frequency signals from entering the LMS algorithm, where an additional feedback cancellation filter and a noise generator is used for providing low-frequency input for the LMS algorithm. The invention also relates to a hearing aid for implementing the method.

WO 01/06812 A1



For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.

TITLE

Feedback cancellation with low frequency input

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TECHNICAL FIELD

The present invention concerns hearing aids. In many hearing aids, for example "In-the-ear" (ITE) and "Behind-the-ear" (BTE), the microphone and the receiver (telephone) components are placed close to each other. This may result in that
10 the sound produced by the receiver leaks back into the microphone. This may occur when the hearing aid shell or the ear mould does not fit sufficiently tight in the ear canal. Given enough amplification in the hearing aid, the loop gain of the system may exceed 0 dB at some frequency and a feedback oscillation may be produced.

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BACKGROUND OF THE INVENTION

The present invention is based on algorithms previously proposed in the literature. The invention concerns a number of algorithm modifications, which
20 overcome some of the limitations of other systems used for feedback reduction in hearing aids.

The invention relates to a feedback cancellation algorithm, which does not need an artificial noise signal in order to estimate the feedback transfer function. The
25 input signal received from the environment, or the feedback oscillation signal, is used to drive the estimation process. In this fashion, the hearing aid user does not listen to an added noise signal, and a higher sound quality is possible. However, it is well known that such 'no-noise' algorithms can have audible side effects under certain circumstances, especially when environmental signals with long
30 autocorrelation functions are present at the microphone.

The autocorrelation function for a signal describes the average correlation between two signal values, which are separated by a time difference "Lag". In loose terms, the autocorrelation function describes how "predictable" a signal

value is, given the other samples in the signal. Some signals, for example periodic signals, are highly predictable and, correspondingly, the autocorrelation function

does not vanish even for large values of Lag. Other signals, such as white noise, are very little predictable, and their autocorrelation function quickly vanish for increasing values of Lag. For signals with a long autocorrelation function, a future sample value can be predicted with a high degree of confidence, given the past samples. In other words, new samples of the signal do not provide much new information. Careful analysis of feedback cancellation systems reveal that signals with long autocorrelation may drive the adaptive system to produce poor estimates of the feedback path.

It is an objective of the present invention to provide a method and a hearing aid having means for feedback cancellation, which improves the result of the feedback canceling by being more stable and thereby gives an improved user comfort.

SUMMARY OF THE INVENTION

According to the invention the first objective is achieved by a method, which comprises the feature of claim 1. According to the invention the first objective is likewise achieved by a hearing aid, which comprises the features of claim 8.

Hereby a more stable system is achieved. The stability is connected with the fact that the LMS algorithm is controlled in a more reliable manner hereby providing more reliable coefficients to the feedback cancellation filter. This results in an improved user comfort.

Advantageous embodiments are described in the dependent claims 2-8 and 10-13. The function and effect of these is explained in connection with the preferred embodiment.

The result of the method and the device is a more reliable feedback detection and hence an improved user comfort.

The present invention includes features, which can eliminate side effects in most cases and improve the adaptation speed resulting in fast suppression of feedback oscillations.

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BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a schematic diagram showing a previously known system used for feedback cancellation;

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FIG. 2 is a schematic diagram showing an embodiment of the system according to the present invention.

FIG. 3 is a schematic diagram showing the feedback detection system according to the invention;

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DETAILED DESCRIPTION OF THE DRAWINGS

A well-known principle for feedback cancellation in hearing aids is shown in fig. 1. All the components described below, except blocks (1), (5) and (50), operate in the discrete time domain.

20

The components are as follows: (1) is a microphone which picks up the sound from the environment (51) ("External input") and the feedback signal (52) ("FBSignal"); (2) is a microphone amplifier and an analog-to-digital converter (A/D); (3) is the hearing aid amplifier with filters, compressors, etc.; (4) is a digital-to-analog converter and a power amplifier; (5) is the hearing aid receiver; (50) is the acoustic feedback path (outside the hearing aid); (6) is a delay unit whose delay matches the delay through the components (4), (5), (50), (1) and (2). (7) is an N-tap finite impulse response (FIR) filter which is intended to simulate the combined impulse response of components (4), (5), (1), (2) and (50). (8) is an adaptive algorithm which will adjust the coefficients (9) of the filter (7) so as to minimize the power of the error signal (10).

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The algorithm (8) is well known as the Least Mean Square (LMS) algorithm. The algorithm requires a reference signal (11), which is used to excite the path consisting of the components (4), (5), (1), (2) and (50). The correlation between the reference signal (11) and the error signal (10) is used to compute the adjustment of the coefficients (9).

The system utilizes the output signal (11) from the hearing aid amplifier block (3) as a driving signal for the LMS algorithm, thereby eliminating the need for a disturbing noise in the receiver (5).

For some external input signals, the LMS based algorithm used in the application shown in fig. 1 is known to have difficulty adjusting the coefficients (9) as desired, i.e. to match the path consisting of components (4), (5), (1), (2) and (50). The difficulties are greatest for signals with long autocorrelation functions.

Mismatched coefficients may lead to audible side effects, which can be very disturbing to a hearing aid user. Those may comprise audible oscillations and change in gain characteristics and frequency characteristics. One general remedy against this problem is to use a low adaptation speed, but this leads to poorer performance of the system because the coefficients cannot track changes in the acoustic feedback path (50) quickly, resulting in a long feedback cancellation time.

The basic system shown in fig. 1 may be improved in various ways to minimize the side effects associated with certain input signals. Many authors have proposed additional system blocks, which will improve the sound quality while maintaining an acceptable adaptation speed.

The present invention is based on the system diagram shown in fig. 1, and the invention consists of additional features, which will improve the sound quality and maintain an acceptable adaptation speed.

FIG.2 shows the block diagram of the general system and the components of the invention.

The embodiment shown includes three features: Adaptation rate control, a frequency-selective adaptation procedure, and a feedback oscillation detector.

Adaptation rate control

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Two well known operation modes for the LMS algorithm are the "standard" mode and the "normalized" mode. In the "standard" mode, the coefficients are updated by an amount that depends on the short-term power of the error signal and the reference signal. This means that the update rate is faster when more powerful
10 signals are processed by the hearing aid. In the "normalized" mode, the update rate is made nearly independent of the signal power, due to a normalization of the update equation.

As described earlier, a low adaptation speed generally improves the sound
15 quality for signals with long autocorrelation functions. In contrast, a high adaptation speed is desirable to reduce feedback oscillations quickly.

Other authors have previously proposed changing the adaptation rate factor (often known as " μ ") when feedback oscillations are detected. Although this does
20 increase the adaptation speed, it also allows coefficients to deteriorate proportionally faster, in those situations where signals with long autocorrelation functions are present at the hearing aid input.

In the present invention, the fact that feedback oscillations often have a high
25 power is used. In many hearing aids, the output level is limited by compressor circuits, and in many cases the maximum output level is well above the normally used output level, for example when speech and other environmental signal are present. It is therefore assumed that the feedback oscillations have a higher power than the environmental signal, in most cases where feedback problems exist.

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Additionally, the feedback oscillation has the desirable property that its frequency is generally equal to the frequency where the loop gain currently is highest, i.e. where the fastest adaptation is needed.

For the reasons mentioned above, it is very effective to utilize the feedback oscillation signal itself as a driving signal for the adaptation.

When the "normalized" adaptation approach is used, the high-power feature of the feedback oscillation is not utilized. If, instead, the "standard" update approach were used, the high power feature of the feedback oscillation would be utilized. At the same time, however, stronger signals in general would cause a higher adaptation speed, which could lead to more autocorrelation problems.

10 The present invention introduces a new normalization scheme, which will generally maintain the low adaptation speed and the normalized operation mode, except when a feedback oscillation is detected. When a feedback oscillation is detected, the system is switched from normalized operation to standard operation by the switch (13), and the full power of the feedback oscillation signal is
15 therefore allowed to adapt the coefficients. During "standard" operation, the update parameter (14) is chosen to such a value (53) that the external input (51) produces approximately the same update rate as it would in "normalized" operation. Assuming that the external input signal (51) maintains nearly constant properties before and during the feedback oscillation, the switch of normalization
20 procedure will be nearly transparent to the external signal (51). This ensures that the sound quality remains high, even though the adaptation speed has been increased due to the higher power in the feedback oscillation. The update parameter (53) to be used during standard mode is estimated in component (12) before the feedback oscillation is detected. During intervals of feedback
25 oscillations, controls signal (15) prevents (12) from updating the parameter (53).

The switch from normalized mode to standard mode may be controlled by a feedback oscillation detector (49) through its output signal (15). The switch (13) may also be controlled by other conditions, which could result in feedback
30 oscillations, for example when the acoustic feedback is rapidly decreased.

The adaptive LMS algorithm (8) may be implemented as the following set of equations:

Normalized operation:

$$h_k(n+1) = h_k(n) + \frac{a \cdot r(n-k) \cdot e(n)}{b + \sum_{p=1}^N r(n)^2}, \quad p = 1..N$$

$$k=1..N \quad (E1)$$

Standard operation:

$$h_k(n+1) = h_k(n) + \frac{a \cdot r(n-k) \cdot e(n)}{b + LT_{sum}}, \quad k = 1..N$$

(E2)

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In these equations, $h_k(n)$ is the k 'th coefficient in the FIR filter at sample time n ; a is a constant which determines the general adaptation speed of the algorithm (this constant is sometimes referred to as " μ "); b is a small constant which prevents division by 0 for very small values of the reference signal; N is the number of coefficients in the filter (7); $r(n)$ is the reference signal (30) sample value at time n ; $e(n)$ is the error signal (28) sample value at time n ; and LT_{sum} is a value computed as described below.

10

15 The sum term of the denominator of E1 is equal to the signal (54). LT_{sum} is equal to the signal (53).

LT_{sum} (equal to (53)), which is computed by component (12), may be updated according to eq. (E3a):

$$LT_{sum}(n+1) = LT_{sum}(n) \cdot \beta_{LT} + SumSq(n) \cdot \alpha_{LT}$$

20

(E3a)

In equation (E3a) $SumSq(n)$ is defined as follows (E3b):

$$SumSq(n) = \sum_{p=1}^N r(n)^2, \quad p = 1..N$$

(E3b)

25 α_{LT} and β_{LT} are time constants, which control the length of the exponential window over which the value of LT_{sum} is computed.

Eq. (E3a) should not be updated while a feedback oscillation is present, since

LT_{sum} should reflect the long-term value of SumSq for segments without oscillation. Once the feedback oscillation has disappeared, eq. (E3a) may be updated again.

In E1 and E3b, the reference signal $r(n)$ is used for normalizing the update equation. However, other signals in the system shown in fig. 2 may also be used instead of $r(n)$. In the literature, the error signal $e(n)$ has been used instead of $r(n)$ for normalization; and even combinations of $r(n)$ and $e(n)$ have been used. The present invention will work for any type of normalization, in which the denominator in E1 and E2 is increased when the power level in the feedback loop consisting of (1), (2), (3), (4), (5) and (50) is increased.

Frequency-selective adaptation

Many feedback cancellation systems proposed earlier contain some form of frequency weighting of the signals which enter the LMS algorithm (8). The purpose of such weighting is to attenuate frequency ranges in which the autocorrelation of the external input signal (51) is long, and thereby reduce the possibility of poorly adjusted coefficients and poor sound quality. Several possibilities exist for frequency weighting. Various combinations of fixed and adaptive filters have been suggested in the past.

In the present invention, steep highpass filters with high attenuation (20) are included in the inputs to the LMS algorithm. The purpose of these filters is to prevent low frequency contents from the reference signal (11) from entering the LMS algorithm. The cutoff frequency for the highpass filters (20) must be lower than the lowest frequency for which feedback cancellation should take place, and otherwise as high as possible.

With the highpass filters (20) in place, the LMS algorithm (8) would not experience an increased level of the error signal (10) when the coefficients (9) are poorly adjusted in the low frequency range. Filter (7) with poorly adjusted

coefficients, combined with components (3) and (6), may lead to a system with a high loop gain, and instabilities may result.

In order to avoid this problem, a parallel feedback cancellation filter (21) is added. This filter is intended to provide low frequency information to the LMS algorithm. The two filters (7) and (21) use identical coefficients (9). While filter (7) is designed to simulate the path consisting of components (4), (5), (1), (2) and (50), filter (21) is designed to simulate the artificial path (25) with an impulse response of constant '0'. The adder (33) computes an error signal as the difference between the desired '0' output and the actual output (34) from the filter (21). The error output (10) from the high frequency range and the error output (27) from the low frequency range are combined into a single error signal (28) which is fed to the error input of the LMS algorithm (8). In order to generate a low frequency signal as input to the filter (21) and to the reference input to the LMS algorithm, a noise generator (22) is included. The noise generator output (29) is lowpass filtered by a fixed filter (23). The cutoff frequency for the lowpass filter (23) is selected approximately equal to the cutoff frequency of the highpass filters (20), to obtain a reasonably flat input spectrum to the LMS algorithm. The low frequency signal (32) and the high frequency signal (31) are combined by the adder (24) to form the complete reference signal (30) for the LMS algorithm. Clearly, the components (25) and (33) may be removed immediately, and the signal (34) can be connected to the signal (27).

The noise generator (22) may be implemented by randomly swapping the numerical sign of each sample of the signal (35). In other words, for each sample instant it is randomly decided whether the sample value should be multiplied by 1 or by (-1). The advantage of using this type of noise generator is that noise samples at (35) and at (29) always have the same amplitude. The power spectrum of the reference signal (30) is therefore reasonably balanced at all times. In the literature, the noise generated as described above is sometimes referred to as 'Schroeder' noise.

Feedback oscillation detector

Feedback oscillations may be produced by a system which contains an amplifier and a feedback loop, under some circumstances. A hearing aid with acoustic amplification, combined with an acoustic path from the hearing aid telephone through a ventilation channel ("vent") and possibly other leaks, form a loop which may have a gain higher than 0 dB, at least for some frequencies. With more than 0 dB loop gain, the system may become unstable and produce feedback oscillations.

The present invention is designed to detect a feedback oscillation in the input signal (55), and set a flag (15) which indicates 'oscillation' or 'no oscillation'.

Some assumptions about the feedback oscillations in hearing aids are included in the design of the detector. The signal produced as a feedback oscillation typically consists of a single frequency, namely the frequency at which the loop gain is highest, taking into account both the linear and non-linear components of the hearing aid. The level of the feedback oscillation is relatively stable, after a certain settling time. The feedback oscillation often dominates the signal in the feedback loop, since its level is often determined by the hearing aid compressors.

The feedback detection process is complicated by the presence of other signals in the feedback loop. Many environmental signals, including music, may contain segments of periodic nature which may resemble a feedback oscillation. However, in the frequency range where oscillations may occur, relatively few environmental signals consist of a single frequency only, at least when considered over a period of a few hundred milliseconds or more.

The feedback oscillation detector in the present invention is based on measuring the overall 'bandwidth' of the signal in the feedback loop consisting of components (1), (2), (3), (4), (5) and (50). In the preferred embodiment, the signal (55) is used as input to the detector, but with slight modifications the detector may obtain its input anywhere in the loop. When the bandwidth of the signal (55) has been small for a certain minimum period of time, the detector will flag a 'feedback oscillation' condition.

FIG. 3 describes the detector (49). The input signal (55) is highpass filtered by an 8-tap FIR filter (36). The filter helps prevent false feedback oscillation detection for low frequency input signals since it suppresses the fundamental frequencies for a wide range of signals. The 3 dB roll-off frequency for the filter should be higher than the lowest expected feedback oscillation frequency. The 8-tap FIR filter is just one example of a usable filter, but many other types may be used. The highpass filtered signal (37) is fed to a modeling device (38), which attempts to model the spectrum of the signal (37), using a second-order auto-regressive model as shown in E4:

$$y(n) = x(n) \cdot K - a_1 y(n-1) - a_2 y(n-2) \quad (E4)$$

where $x(n)$ represents the excitation signal, which drives the model input, while $y(n)$ is the output from the model.

The signal model E4 represents a second-order IIR filter with a single complex-conjugated pole-pair. Based on the model coefficients a_1 and a_2 (39), the filters center frequency and bandwidth may be computed. This computation is performed by the unit (40), which produces a bandwidth (41) and a center frequency (48). These two values are compared by (47) to preset thresholds (43) and (46). The comparator sets flag (44) TRUE if the bandwidth (41) is lower than the preset threshold (43) AND the center frequency (48) is higher than the acceptable minimum feedback oscillation frequency (46). Otherwise the flag (44) is set FALSE.

All components (38), (40), (47) and (45) are working on a frame based schedule. A frame length of 40 ms may be used, but other values of the length would also work. For each frame, a new value of the flag (44) is computed. Since many environmental input signals contain short segments of narrow bandwidth, the flag (44) may occasionally be set TRUE while no feedback oscillations are present. To avoid this, the flag (44) is fed to a stability estimator (45). In here, the flag (44) is placed in a delay line which, at any point in time, holds the values of the flag from the last N_{se} frames. N_{se} may be selected as 10, but other values would also work. The stability estimator (45) sets the detector flag (15) TRUE when and

only when at least N_{\min} out of the N_{past} past values of the flag (44) were TRUE. For example, N_{\min} may be set to 4.

The coefficients a_1 and a_2 in E4 are computed from the autocorrelation coefficients $R(0)$, $R(1)$ and $R(2)$, by solving the equations:

$$R(0) \cdot a_1 + R(1) \cdot a_2 = -R(1) \quad (\text{E5a})$$

$$R(1) \cdot a_1 + R(0) \cdot a_2 = -R(2) \quad (\text{E5b})$$

The autocorrelation coefficients may be computed using the following equations:

$$R(0) = \frac{1}{N_f} \cdot \sum x(n)^2, \quad n = 1..N_f \quad (\text{E6a})$$

$$R(1) = \frac{1}{N_f} \cdot \sum x(n) \cdot x(n+1), \quad n = 1..N_f - 1 \quad (\text{E6b})$$

$$R(2) = \frac{1}{N_f} \cdot \sum x(n) \cdot x(n+2), \quad n = 1..N_f - 2 \quad (\text{E6c})$$

where N_f corresponds to the frame length, and $x(i)$ is the i 'th sample of signal (37) from the current frame.

The 3-dB bandwidth of the filter represented by the auto-regressive model E4 may be computed as

$$\text{Bandwidth} = 2 \cdot (1 - \sqrt{a_2}) \quad (\text{E7})$$

and the center frequency may be computed as

$$f_{\text{center}} = \cos^{-1}\left(\frac{-a_1}{2\sqrt{a_2}}\right) \quad (\text{E8})$$

In both equations (E7) and (E8) the result is given in radians. Simple calculations, in which the system sample rate is included, may be used to convert the values of Bandwidth and the f_{Center} into Hz.

5

In the previous description the hearing aid and the methods have been described in a simplified manner. Necessary elements like a power source, e.g. a battery, and related wiring, the signal processing capabilities of the hearing aid amplifier and the interconnecting wiring of the components, as well as the housing, which is always present have been omitted from the general definition of the hearing aid according to the invention. It should be appreciated that these elements of course are present in a hearing aid actually manufactured.

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14
CLAIMS

1. A method for canceling feedback in an acoustic system comprising a microphone, a signal path, a speaker, means for detecting presence of
5 feedback between the speaker and the microphone and filter means for compensating at least partly a possible feedback signal, the method comprising:
 - using a LMS algorithm for generating filter coefficients ;
 - using a highpass filter to prevent low-frequency signals from entering the
10 LMS algorithm;
 - where an additional feedback cancellation filter and a noise generator is used for providing low-frequency input for the LMS algorithm.
2. A method according to claim 1, where a sign-swapping algorithm is used for
15 generating a broad band noise signal, having an amplitude substantially equal to the amplitude of the signal from which it was derived.
3. A method according to any of the claims 1 or 2 where a steep low pass filter is used generate a low frequency noise signal to be used as an additional input
20 to the LMS algorithm.
4. A method according to claim 1, where the LMS algorithm operates with a predetermined essentially level independent adaptation speed when feedback is not present, this representing a first mode,
25
 - where the LMS algorithm operates a level dependent adaptation speed when feedback is present, this representing a second mode;
 - where the means for detecting the presence of feedback is used to control the adaptation mode selection of the LMS algorithm;
 - where the update rate for the LMS algorithm is determined by the long-
30 term average denominator in the LMS update algorithm in the second mode.
5. A method according to any of the claims 1-4, comprising a microphone, a signal path, a speaker, means for detecting presence of feedback between the

speaker and the microphone and filter means for at least partly compensating a possible feedback signal, the method comprising:

- using bandwidth detection means for determining the presence of a feedback signal.

5

6. A method according to any of the claims 1-5, where the stability of the signal determined as a feedback signal is analyzed.

10

7. A method according to any of the claims 1-6, where the feedback analyzing comprises holding flag values from a number of succeeding time frames and comparing of these.

15

8. A method for canceling feedback in an acoustic system comprising a microphone, a signal path, a speaker, means for detecting presence of feedback between the speaker and the microphone and filter means for compensating at least partly a possible feedback signal, the method comprising:

20

- using a LMS algorithm for generating filter coefficients ;
- using a highpass filter to prevent low-frequency signals from entering the LMS algorithm;

25

9. A hearing aid comprising :

- a microphone;
- a signal path;
- an amplifier;
- a speaker;
- means for detecting feedback between the speaker and the microphone;
- filter means for at least partly compensating a possible feedback signal;
- memory means including a LMS algorithm for generating filter coefficients;
- at least one highpass filter for preventing low-frequency signals from entering the LMS algorithm;
- an additional feedback cancellation filter and a noise generator for providing low-frequency input for the LMS algorithm.

30

10. A hearing aid according to claim 8, further comprising steep low pass filters for generating a low frequency noise signal to be used as an additional input to the LMS algorithm.

5

11. A hearing aid comprising :

- a microphone;
- a signal path;
- an amplifier;
- 10 - a speaker;
- means for detecting feedback between the speaker and the microphone;
- filter means for at least partly compensating a possible feedback signal;
- memory means including a LMS algorithm for generating filter coefficients;
- 15 - where the means for detecting feedback include a bandwidth detecting means.

12. A hearing aid according to claim 10, further comprising a stability detector for the signal determined as a feedback signal.

20

13. A hearing aid according to claim 11, where the stability detector comprises storage means for a number of values from a number of succeeding time frames and means for comparing these.

25

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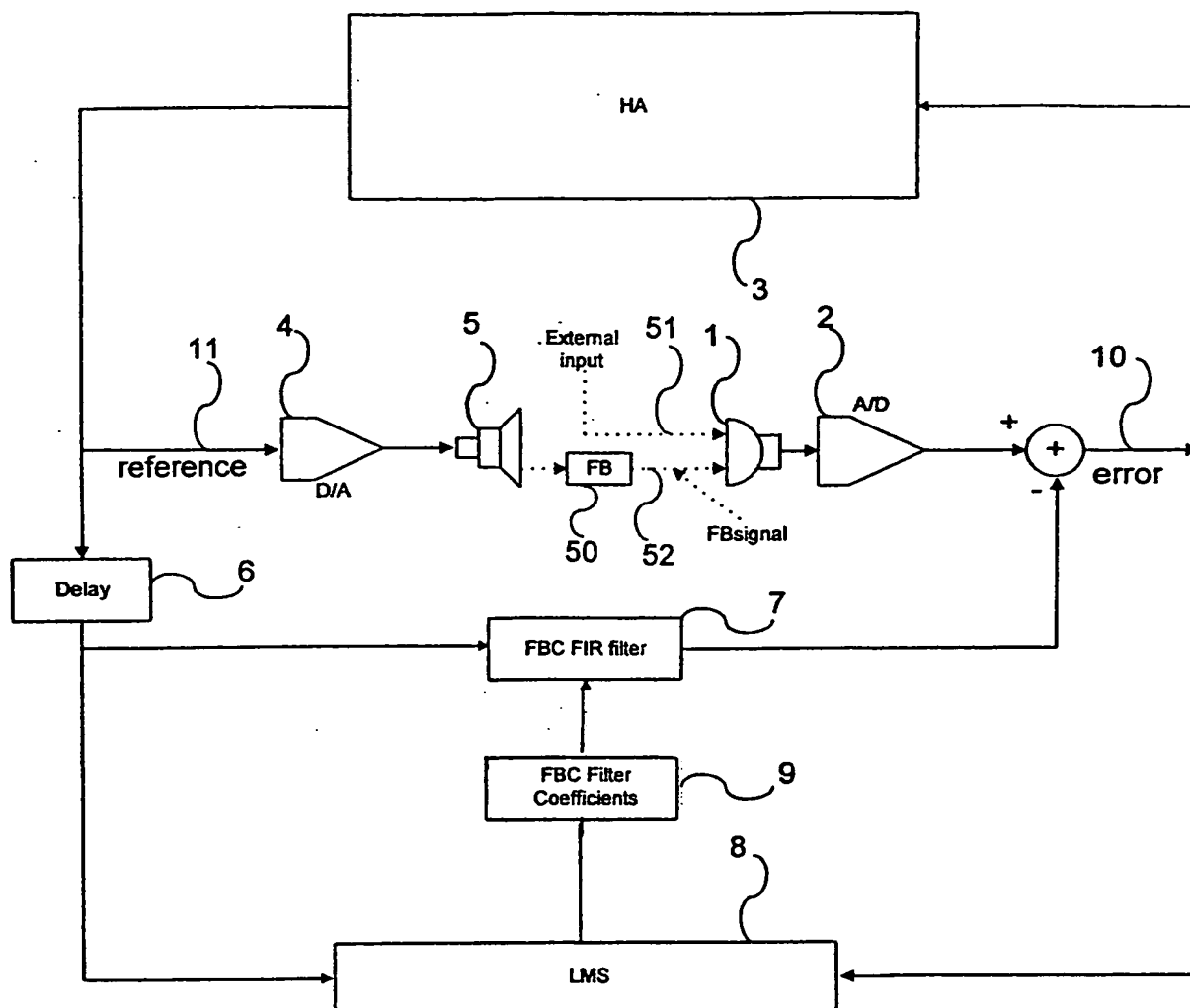


Fig. 1

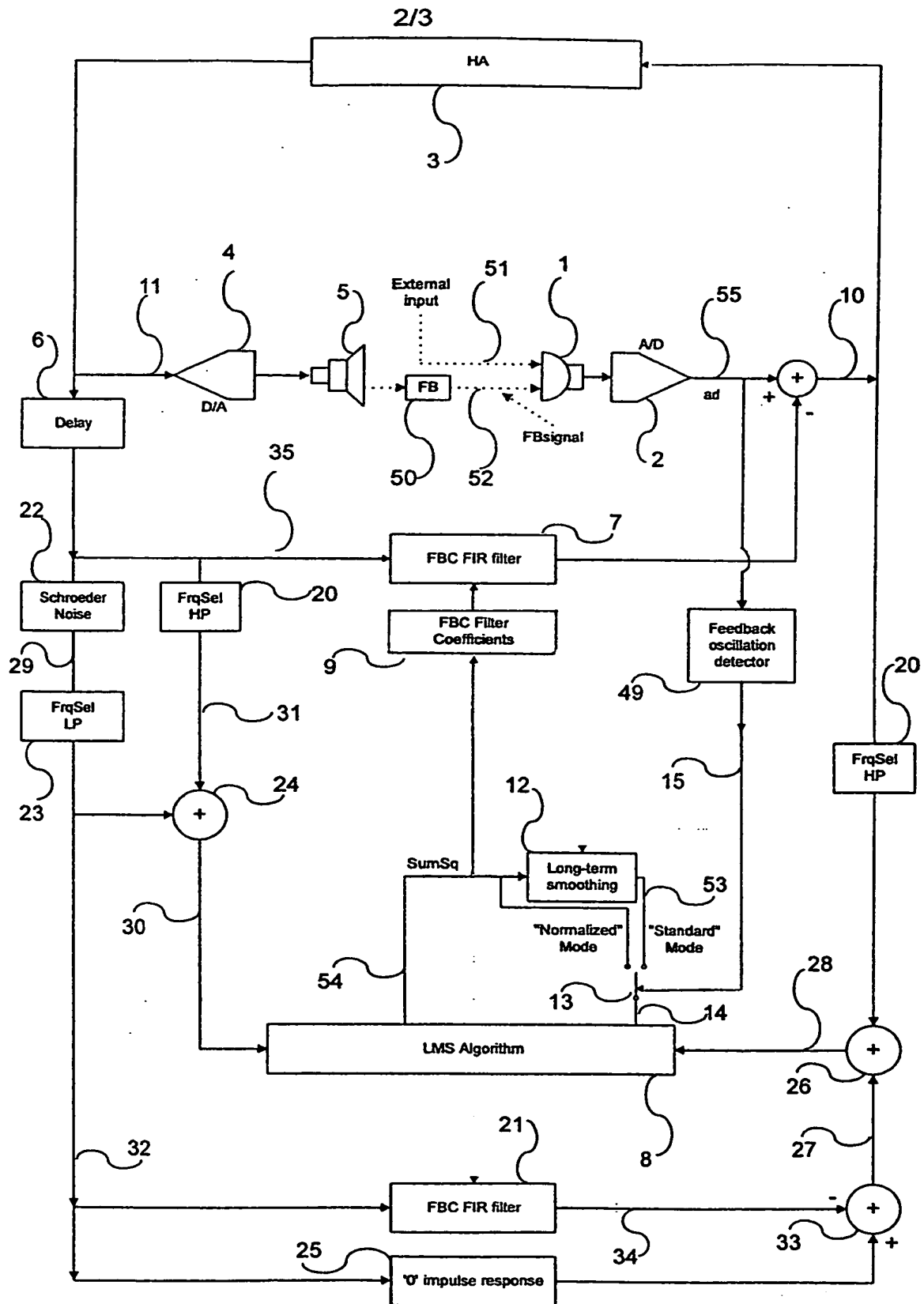


Fig. 2

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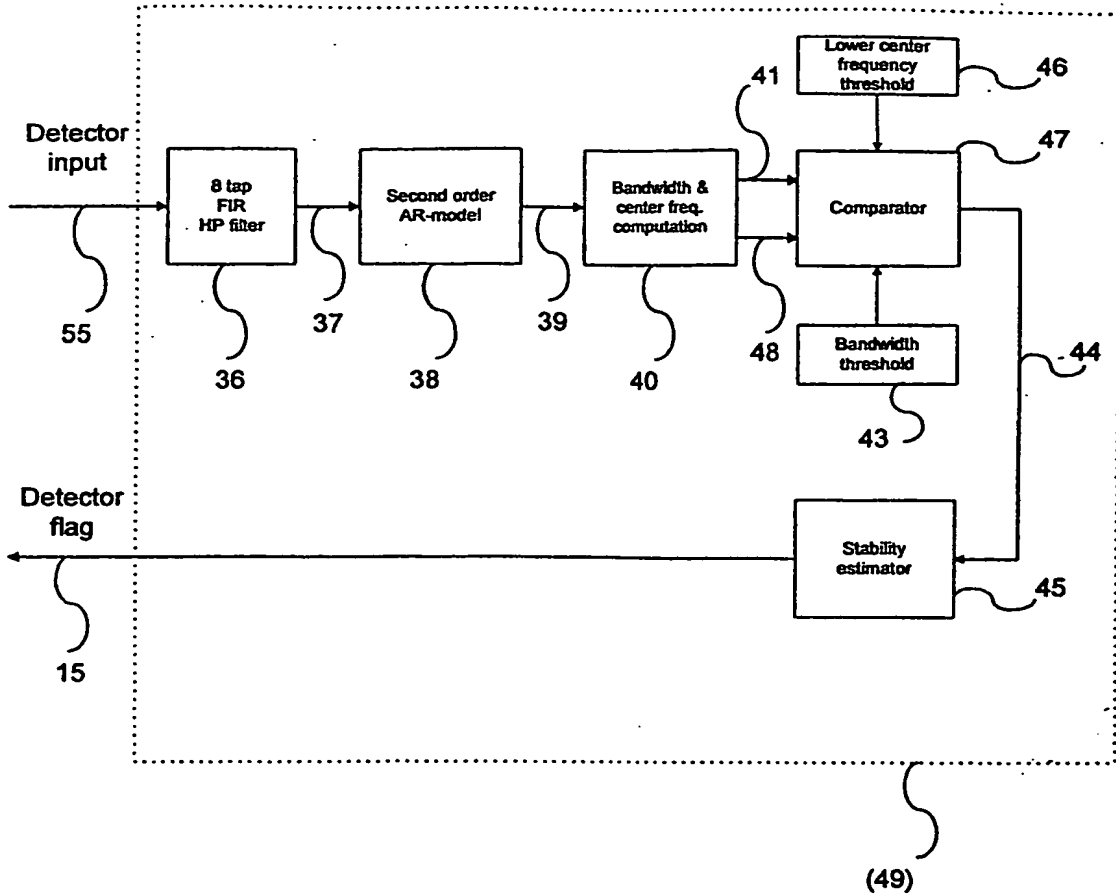


Fig. 3

PATENT COOPERATION TREATY

PCT

REC'D 29 OCT 2001

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INTERNATIONAL PRELIMINARY EXAMINATION REPORT

(PCT Article 36 and Rule 70)



5

Applicant's or agent's file reference P-1999-014-2	FOR FURTHER ACTION See Notification of Transmittal of International Preliminary Examination Report (Form PCT/IPEA/416)	
International application No. PCT/DK00/00380	International filing date (day/month/year) 07/07/2000	Priority date (day/month/year) 19/07/1999
International Patent Classification (IPC) or national classification and IPC H04R25/00		
Applicant OTICON A/S et al.		

1. This international preliminary examination report has been prepared by this International Preliminary Examining Authority and is transmitted to the applicant according to Article 36.
2. This REPORT consists of a total of 5 sheets, including this cover sheet.
 - ☒ This report is also accompanied by ANNEXES, i.e. sheets of the description, claims and/or drawings which have been amended and are the basis for this report and/or sheets containing rectifications made before this Authority (see Rule 70.16 and Section 607 of the Administrative Instructions under the PCT).

These annexes consist of a total of 2 sheets.

3. This report contains indications relating to the following items:
 - I ☒ Basis of the report
 - II ☐ Priority
 - III ☐ Non-establishment of opinion with regard to novelty, inventive step and industrial applicability
 - IV ☐ Lack of unity of invention
 - V ☒ Reasoned statement under Article 35(2) with regard to novelty, inventive step or industrial applicability; citations and explanations supporting such statement
 - VI ☐ Certain documents cited
 - VII ☒ Certain defects in the international application
 - VIII ☒ Certain observations on the international application

Date of submission of the demand 19/02/2001	Date of completion of this report 24.10.2001
Name and mailing address of the international preliminary examining authority:  European Patent Office D-80298 Munich Tel. +49 89 2399 - 0 Tx: 523656 epmu d Fax: +49 89 2399 - 4465	Authorized officer Fribert, J Telephone No. +49 89 2399 8959 

**INTERNATIONAL PRELIMINARY
EXAMINATION REPORT**

International application No. PCT/DK00/00380

I. Basis of the report

1. With regard to the **elements** of the international application (*Replacement sheets which have been furnished to the receiving Office in response to an invitation under Article 14 are referred to in this report as "originally filed" and are not annexed to this report since they do not contain amendments (Rules 70.16 and 70.17)*):

Description, pages:

1-13 as originally filed

Claims, No.:

1-9 with telefax of 20/08/2001

Drawings, sheets:

1/3-3/3 as originally filed

2. With regard to the **language**, all the elements marked above were available or furnished to this Authority in the language in which the international application was filed, unless otherwise indicated under this item.

These elements were available or furnished to this Authority in the following language: , which is:

- ☐ the language of a translation furnished for the purposes of the international search (under Rule 23.1(b)).
- ☐ the language of publication of the international application (under Rule 48.3(b)).
- ☐ the language of a translation furnished for the purposes of international preliminary examination (under Rule 55.2 and/or 55.3).

3. With regard to any **nucleotide and/or amino acid sequence** disclosed in the international application, the international preliminary examination was carried out on the basis of the sequence listing:

- ☐ contained in the international application in written form.
- ☐ filed together with the international application in computer readable form.
- ☐ furnished subsequently to this Authority in written form.
- ☐ furnished subsequently to this Authority in computer readable form.
- ☐ The statement that the subsequently furnished written sequence listing does not go beyond the disclosure in the international application as filed has been furnished.
- ☐ The statement that the information recorded in computer readable form is identical to the written sequence listing has been furnished.

4. The amendments have resulted in the cancellation of:

- ☐ the description, pages:
- ☒ the claims, Nos.: 10-13

**INTERNATIONAL PRELIMINARY
EXAMINATION REPORT**

International application No. PCT/DK00/00380

☐ the drawings, sheets:

5. ☐ This report has been established as if (some of) the amendments had not been made, since they have been considered to go beyond the disclosure as filed (Rule 70.2(c)):

(Any replacement sheet containing such amendments must be referred to under item 1 and annexed to this report.)

6. Additional observations, if necessary:

V. Reasoned statement under Article 35(2) with regard to novelty, inventive step or industrial applicability; citations and explanations supporting such statement

1. Statement

Novelty (N)	Yes: Claims 1-9
	No: Claims
Inventive step (IS)	Yes: Claims 1-9
	No: Claims
Industrial applicability (IA)	Yes: Claims 1-9
	No: Claims

- 2. Citations and explanations**
see separate sheet

VII. Certain defects in the international application

The following defects in the form or contents of the international application have been noted:
see separate sheet

VIII. Certain observations on the international application

The following observations on the clarity of the claims, description, and drawings or on the question whether the claims are fully supported by the description, are made:
see separate sheet

Re Item V

Reasoned statement under Article 35(2) with regard to novelty, inventive step or industrial applicability; citations and explanations supporting such statement

1. In order to assess novelty, inventive step and industrial applicability of the claims, the obscurities in claims 1 and 8 mentioned in Section VIII below has been interpreted in the light of the description, to mean that the high pass filters prevent low frequency signals contained in the speaker signal from entering the LMS algorithm while low frequency signals from the feedback cancellation filter and the noise generator can be input to the LMS algorithm.
2. The closest prior art is described on pages 1 and 2 of the description and is shown in Fig. 1.
3. Object: To provide a method and a hearing aid having means for feedback cancellation, which improves the result of the feedback cancelling by being more stable and thereby gives an improved user comfort.
4. Solution: Provision of a high pass filter preventing low frequency signals contained in the speaker signal from entering the LMS algorithm while low frequency signals from the feedback cancellation filter and the noise generator can be input to the LMS algorithm.
5. These features are not known from any of the prior art documents of the search report and are thus not rendered obvious. Thus, there is no hint in the prior art to enable the person skilled in the art to arrive at a method according to claim 1 or a hearing aid according to claim 8 without the exercise of inventive skill.

The advantage of the invention is that the LMS algorithm is controlled in a more reliable manner hereby providing more reliable coefficients to the feedback cancellation filter.

6. Claims 1 and 8 equals original claims 1 and 9 respectively.

**INTERNATIONAL PRELIMINARY
EXAMINATION REPORT - SEPARATE SHEET**

International application No. PCT/DK00/00380

7. Claims 2 to 7 and 9 are dependent on claims 1 and 8, respectively and as such also meet the requirements of the PCT with respect to novelty and inventive step.

Re Item VII

Certain defects in the international application

1. The features of the claims are not provided with reference signs placed in parentheses (Rule 6.2(b) PCT).
2. The description page 2, lines 19-21 and 28-30 has not been adapted to the amended claims.

Re Item VIII

Certain observations on the international application

1. The claims are not clear and concise contrary to Article 6 PCT for the following reasons:
 - (a) The wording of claim 1 is obscure, due to the fact that it first claims a high pass filter preventing low-frequency signals entering the algorithm and then claims a filter and a noise generator providing low frequency signals to the algorithm.
 - (b) This objection is also valid against independent claim 8.

CLAIMS

1. A method for canceling feedback in an acoustic system comprising a microphone, a signal path, a speaker, means for detecting presence of feedback between the speaker and the microphone and filter means for compensating at least partly a possible feedback signal, the method comprising:
- 5
- using a LMS algorithm for generating filter coefficients
 - using a highpass filter to prevent low-frequency signals from entering the LMS algorithm;
 - where an additional feedback cancellation filter and a noise generator is

10 used for providing low-frequency input for the LMS algorithm.
2. A method according to claim 1, where a sign-swapping algorithm is used for generating a broad band noise signal, having an amplitude substantially equal to the amplitude of the signal from which it was derived.
- 15
3. A method according to any of the claims 1 or 2 where a steep low pass filter is used generate a low frequency noise signal to be used as an additional input to the LMS algorithm.
- 20
4. A method according to claim 1, where the LMS algorithm operates with a predetermined essentially level independent adaptation speed when feedback is not present, this representing a first mode
- where the LMS algorithm operates a level dependent adaptation speed when feedback is present, this representing a second mode;

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 - where the means for detecting the presence of feedback is used to control the adaptation mode selection of the LMS algorithm;
 - where the update rate for the LMS algorithm is determined by the long-term average denominator in the LMS update algorithm in the second mode.

30
5. A method according to any of the claims 1-4, comprising a microphone, a signal path, a speaker, means for detecting presence of feedback between the speaker and the microphone and filter means for at least partly compensating a possible feedback signal, the method comprising:

- using bandwidth detection means for determining the presence of a feedback signal.

- 5 6. A method according to any of the claims 1-5, where the stability of the signal determined as a feedback signal is analyzed.
7. A method according to any of the claims 1-6, where the feedback analyzing comprises holding flag values from a number of succeeding time frames and comparing of these.
- 10 8. A hearing aid comprising:
- a microphone;
 - a signal path;
 - an amplifier;
 - 15 - a speaker;
 - means for detecting feedback between the speaker and the microphone;
 - filter means for at least partly compensating a possible feedback signal;
 - memory means including a LMS algorithm for generating filter coefficients;
 - at least one highpass filter for preventing low-frequency signals from
 - 20 entering the LMS algorithm;
 - an additional feedback cancellation filter and a noise generator for providing low-frequency input for the LMS algorithm.
9. A hearing aid according to claim 8, further comprising steep low pass filters
- 25 for generating a low frequency noise signal to be used as an additional input to the LMS algorithm.